

# Power- and Delay-Aware Mobile Application-Data Flow Adaptation: the MobiHealth System Case Study<sup>1</sup>

Katarzyna Wac, Mortaza Bargh, Arjan Peddemors, Pravin Pawar, Bert-Jan van Beijnum, Richard Bults

**Abstract.** Emerging healthcare applications rely on personal mobile devices to monitor patient vital signs and to send it to the hospitals-backend servers for further analysis. However, these devices have limited resources that must be used optimally in order to meet the requirements of healthcare applications end-users: healthcare professionals and their patients. This paper reports on a case study of a cardiac telemonitoring application delivered by the so-called MobiHealth system. This system relies on a commercial device with multiple (wireless) network interfaces (NI). Our study focuses on how the choice of a NI affects the end-to-end application's data delay (extremely important in case of patient's emergency) and the energy consumption of the device (relating to the service sustainability while a patient is mobile). Our results show the trade-off between the delay and battery savings achieved by various NI activation strategies in combination with application-data flow adaptation. For a given mobile device, our study shows a gain of 40-90% in battery savings, traded against the higher delays (therefore applicable mainly in non-emergency cases). The insights of our studies can be used for application-data flow adaptation aiming at battery saving and prolonging device's operation for mobile patients.

**Keywords**-mobile device connectivity management; energy efficiency; end-to-end delay; application adaptation; mobile healthcare

## 1 Introduction

The emergence of new wireless broadband networks and the increased diversity of miniaturized and personalized networked devices give rise to a variety of new mobile interactive applications in our daily life. Examples of these are, on one hand, applications supporting traditional users as information-*consumers*, e.g. news, leisure and entertainment content delivery. On the other hand, mobile users are no longer only passive information and content consumers, but on a growing scale they take the role of content *producers*. Examples of these applications are especially ones supporting social networking. However, another emerging application domain, in which a user acts as a content producer, is a mobile healthcare domain, where a mobile patient's vital signs can be telemonitored by his healthcare professional in the healthcare center. In this paper we focus on this application example.

The above mentioned applications are ultimately envisaged to be delivered to the user on the move: anywhere anytime and under different conditions, while

---

<sup>1</sup> This work is part of the Dutch Freeband AWARENESS project (<http://awareness.freeband.nl>, contract BSIK 03025)

fulfilling his *Quality of Service (QoS) requirements*. These requirements are, e.g., low application delays, long device battery life and seamless user mobility support along with low monetary cost of networks usage. However, as applications operate in a heterogeneous networking environment, consisting of a variety of wireless and wired networks owned by different parties, the QoS provided by this environment is one of the most critical factors influencing the assurance of the QoS provided by the application to the user. In this paper, the *QoS provided* by an *application* is defined as an *application-level throughput* (in kbps) and an *application-level delay* (in milliseconds).

There exists close relation between the provided application-level QoS and the provided network-level QoS. Particularly, the provided application-level throughput and delay depend respectively on throughput and data delay while using particular underlying (wireless) network over the given network interface (NI) on the mobile device. Moreover, the device battery life depends on a given application, given NI, and on how *application-data flow* is offered to this NI. Particularly, this flow is described in terms of its volume, i.e., size and rate of the data offered to the NI. By changing the size and the rate parameters we change volume of data to be sent; in such a way we can adapt the application-data flow to suit better the provided network-level QoS and to obtain better application-level QoS.

This paper focuses on 1) an choice of NI (as available on a mobile device) and its activation strategy (ON/OFF) and 2) an application-data flow adaptation, and relations of these two with a) a device's energy consumption and b) an application-data delay. In this paper we study the relation of these four parameters to the user's required QoS for a health telemonitoring application [1], and particularly, cardiac telemonitoring application delivered by the so-called MobiHealth system [2].

The rest of this paper is organized as follows. Section 2 provides a description of the MobiHealth system, while 3 - a mobile device's NI states and their selection criteria. Section 4 provides our measurement methodology for energy and delay measurements for a commercial mobile device used in the MobiHealth system. Section 5 analyzes the measurement results, based on which we defined NI activation strategies. R Section 6 discusses related work. Based on measurements results, in Section 7 we provide the conclusions and recommendations for the MobiHealth system usage and some future work areas.

## **2 The MobiHealth system**

### **2.1 System Overview**

The MobiHealth system is a distributed system for telemonitoring of a patient's health condition.

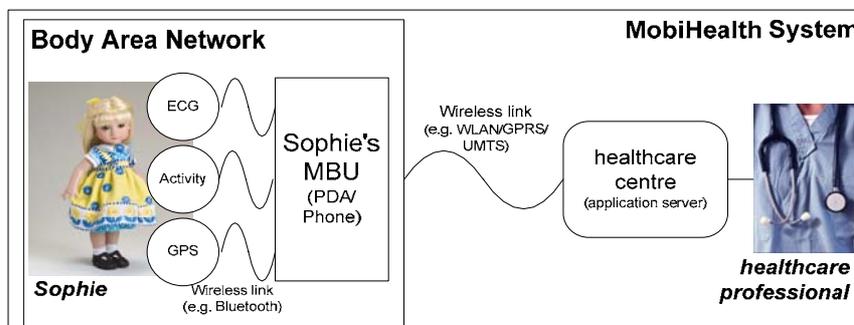


Figure. 1 MobiHealth system overview.

In the MobiHealth system (Fig. 1), a patient is wearing a *Body Area Network* (BAN), consisting of a sensor-set and a *Mobile Base Unit* (MBU). The sensor-set consists of specialized sensors monitoring the patient's vital signs, an alarm button, to be pressed by the patient in emergency, and a location-determination sensor (e.g. a GPS). The sensor-set is specific for a patient's health condition, e.g. respiration insufficiency, cardiac problems, and epilepsy. Emergency condition is defined individually for each patient, based on his/her health condition. It can be activated based on a) patient's pressing the alarm button or, based on the patient's vital signs analysis on b) the BAN or c) the backend-server.

The MBU is the central unit of a BAN, usually in the form of a mobile phone or PDA. It continuously collects sensor data, processes it (e.g. filters, shapes, correlates) and sends in real-time to a remote application *backend-server* located in a healthcare center, where it can be made available for e.g., medical decision support systems.

The BAN uses the intra-BAN communication network, e.g. Bluetooth (BT) to send data from the sensor-set to the MBU, and an extra-BAN communication network, e.g. WLAN or 2.5G/3G (i.e. GPRS/UMTS) for exchange of the application and control data between the MBU and the backend-server.

The application execution is supported by a proprietary *MSP-Interconnect protocol (MSP-IP)* [3]; a TCP/IP-stack-based protocol, facilitating application-data-plane and control-plane<sup>2</sup> data. The overall system architecture conforms the Jini Interconnect specifications as we presented in [4]. Detailed description of the MobiHealth system we presented in [2, 5].

## 2.2 Telemonitoring Application-Data Flow

In this paper, we consider the telemonitoring application for cardiac patients in a non-critical condition, i.e., with a small probability of an emergency. Hence we consider application-data flow adaptation cases separately for an emergency and non-emergency (Section 2.C).

<sup>2</sup> BAN control-plane data consists of the MBU management lifecycle and aliveness (Keep-Alive) messages

The sensor-set acquires patient's heartrate (HR), oxygen saturation (SO<sub>2</sub>) and plethysmogram (pleth), an alarm button state, and a control-data. Sensors sampling frequency is 128Hz; each sample consists of a 5B of application-data. A unit of data that the application collects consists of 1s aggregated sensor-set data, so, in total of 640 B. Every unit of data is compressed (lossless) before being sent by the extra-BAN communication network. The data compression factor, i.e., the reduction in size relative to the uncompressed size, is 80-85 %. However, this factor strongly depends on the actual values of the measured vital signs; it decreases with increased variability in measured vital signs. The MSP-IP introduces a 10 B overhead per an aggregated and compressed data. Hence, the protocol stack overhead is 64 B for WLAN (MSP-IP/TCP/IP/Ethernet) and 58 B for GPRS (MSP-IP/TCP/IP/PPP). The resulting data unit is sent over the data-plane. The overall volume of data sent by the NI contains data-plane and control-plane<sup>3</sup> data; ~1.2-1.5 kbps<sup>4</sup>.

### 2.3 QoS Requirements

The end-users of the telemonitoring applications are healthcare professionals are their patients. Only the former ones are in charge to define the QoS requirements [6]. These requirements are related to application-data exchange performance a) its reliability (lossless and error-free) and b) a minimum application-data delay (in case of a patient's emergency) from the sensor-set to the backend-server. The use of TCP/IP protocol stack and the use of local data storage in case when no network is available to send the data or a real-time sending is not required, ensure system recovery in case of data loss and encountered data-errors. Further study of application reliability is outside of scope of this paper.

Concerning the application-data delay requirement, we focus on the extra-BAN data delay, as a major contributor to the application-data delay in the MobiHealth system. Particularly the MobiHealth system performance is managed based on an *application-level Round Trip Response* (AppRTT)<sup>5</sup> times. The AppRTT is a time period it takes for a control message (i.e., a MBU Keep-Alive<sup>6</sup> [4]) originated from the MBU, to be bounced by the backend-server (without being processed there) and received back by the MBU. AppRTT strongly depends on the choice of the extra-BAN communication network, i.e. the NI choice at the MBU, and the volume of the application-data being sent. Moreover, The AppRTT reflects the delays provided by the underlying networks, as it is composed of the processing delays in the protocol stacks at the MBU and the backend-server side as well as an uplink (MBU to the backend-server) and downlink (backend-server to the MBU) network delays.

<sup>3</sup> of a negligible size comparing to the data-plane

<sup>4</sup> Data-plane calculation for compression factor of 80%: a) WLAN:  $[(640 * 0.2) + 64] * 8$  bps = 1536 bps b) GPRS:  $[(640 * 0.2) + 58] * 8$  bps = 1488 bps;

Data-plane calculation for compression factor of 85%: a) WLAN:  $[(640 * 0.15) + 64] * 8$  bps = 1280 bps b) GPRS:  $[(640 * 0.15) + 58] * 8$  bps = 1232 bps

<sup>5</sup> Reliable one-way delay measurements are only possible if the clocks of MBU and backend-server would be synchronized; it is hardly feasible in the operational system

<sup>6</sup> KeepAlive message of size of 41 B

The considered cardiac telemonitoring application's delay requirements strongly depend on the actual health condition of a patient. In emergency, patient vital signs data needs to be continuously sent (at a minimum possible delay) to the backend-server, where it is made available for a healthcare professional in real-time. For non-emergency, it is possible that the MBU acquires the application-data (for data-plane and control-plane), stores it locally, and sends it to the backend-server later (i.e., in bursts), e.g. when a cheap, high-throughput WLAN network is available. It is also possible that in non-emergency, the (real-time) BAN data is sent continuously to the backend-server along with the previously stored BAN data.

Another QoS requirement for MobiHealth is a maximum lifetime of the BAN. In this paper we focus on the MBU's power consumption for extra-BAN communication, as its contribution to the BAN's power consumption. We denote the MBU power consumption as  $power_{MBU}$ . It depends on the NI used for extra-BAN communication and the volume of the application-data being sent.

In our study we also consider an additional user's requirement resulting from the fact that a patient needs to use his MBU as a regular (WWAN) phone and needs to be WWAN-*reachable*, especially by his healthcare professional, for voice/data communication. Assurance of this requirement may not be favorable from the power perspective<sup>7</sup>; however in our study we consider this requirement.

We note additionally, that the MBU power consumption depends also on a user's mobility level and the MBU configuration parameters e.g. backlight level, other running applications, or MBU location with respect to the network's access point/base station (i.e., MBU's received signal strength). However, in our study, we assume that a patient wearing BAN is in a fixed location (i.e. not being mobile).

### 3 Network Interfaces Activation

#### 3.1 Network Interface States

The existing wireless technologies accessible by commercial mobile devices can be divided into two categories: WWANs that provide a low-throughput and high-delay service over a wide geographic area (e.g. GPRS or UMTS) and WLANs that provide a high-throughput and low delay service over a narrow geographic area (e.g. WiFi) [7]. We consider a device NI state model for mobile devices with GPRS or/and UMTS as WWAN interface and WiFi as WLAN interface. A NI is in one of the following states: 1) OFF 2) ON-IDLE: an IP-idle state, where the mobile device has IP connectivity to the Internet. However it does not send/receive application level data-plane or control-plane IP packets (i.e., IP packets carrying application-data) or 3) ON-ACTIVE: an IP-active state, where mobile device is sending or receiving application level IP packets through this NI.

From the telemonitoring application perspective, application data can be send 1) via the WLAN and WWAN NIs 2) via the WLAN NI, while the WWAN NI is OFF or ON-IDLE or 3) via the WWAN NI, while the WLAN NI is OFF or ON-

---

<sup>7</sup> Additional power is consumed if WWAN is in ON-IDLE state without sending data

IDLE or 4) or being stored locally, while the WWAN (or WLAN) NI is OFF or ON-IDLE. Note that the NI that is used to send data could be in ON-ACTIVE state continuously or could alternate between the ON-ACTIVE and the ON-IDLE/OFF states (the latter implies data send in bursts).

### 3.2 Criteria for a Choice of a NI State

Based on the scope of our study and on the requirements posed by the MobiHealth users (Section 2.C), we conclude that a NI state (i.e., OFF/ON-IDLE/ON-ACTIVE) depends on criteria (i) application-data delay requirement posed by the current health condition of a patient (i.e., emergency or non-emergency) (ii) the power<sub>MBU</sub> consumption while using that NI and (iii) the provided AppRTT while using that NI.

## 4 Measurements

### 4.1 MobiHealth System Setup

The MobiHealth sensor-set is based on Mobi5-3e1as [8], with only the NONIN finger clip attached (for HR, SO<sub>2</sub> and pleth data). As a MBU we have used Qtek 9090 with Intel® PXA263 400 MHz processor (32b), 128 MB RAM, firmware version 1.31.00 WWE (from 13.12.2004), radio version 1.06.02, protocol version 1337.38 running Windows Mobile 2003 SE PocketPC OS edition version 4.21.1088. The Qtek's battery is of a standard type, rechargeable Li-ion Polymer of capacity of 1490 mAh (3.7V, model PH26B). The Qtek has a TFT touch screen display of size of 53x71 mm (214 x 320 pixels, 65K colors) and its backlight level was set to zero.

The MBU has the WWAN-GPRS (GSM 850/900/ 1800/1900 Hz, class 10: 4+1/3+2 slots) and WLAN-WiFi (IEEE 802.11b, with 'best-battery' setting in the OS) as NIs for extra-BAN communication. The BT NI is used continuously for intra-BAN communication for sensor-set data acquisition. The MBU uses GPRS network provided by Sunrise mobile operator (received signal strength of 100%) and WLAN provided by the University of Geneva, Switzerland (received signal strength of 50%), where the MBU was placed such that the received signal strength has been maximized along the measurements). The backend-server used is a standard high-performance server dedicated to MobiHealth telemonitoring services. The server was placed at Twente University, the Netherlands. The MobiHealth telemonitoring application software version is a release from 17 October 2007.

#### 4.1.2 Power and delay measurements instrumentation

The MobiHealth system was configured such that during the execution of the telemonitoring application, we collected the measurements logs at the MBU and backend-server. To measure the energy consumption of the MBU, we logged the remaining battery percentage in 5 seconds intervals. For the purpose of delay

measurements, the MBU was instructed to log the AppRTT in intervals of 10 seconds continuously along the telemonitoring application delivery.

To obtain high application-data flow volumes, not feasible in the current state of the MobiHealth system, and especially important for our measurements over (high-throughput) WLAN NI (cases 3 and 4); we have used the NetPerf application [9]. This application is generating TCP traffic and measuring a unidirectional throughput between the MBU and the backend-server. These measurements were done for the same conditions as the other measurements; however, the MobiHealth application was NOT running in the background of the NetPerf application. By using this application, we attempted to simulate a case where MBU sends previously stored patient vital signs data. In the NetPerf measurements we obtained only the  $power_{MBU}$  values.

Along the measurements, we assumed the MobiHealth system to be in the steady-state representing the behavior of the system usage for a typical system user, i.e. a cardiac patient, whose vital signs are being monitored. Measurements have been done over a time span of two weeks, always at same location (our University of Geneva office) but at different hours.

#### 4.2 Measurements Cases

For the purpose of our research, we considered various measurements cases based on the following two parameters: application-data flow and NIs states. Each case represents the combination of states of the MBU WLAN and GPRS NIs (and BT ON-ACTIVE for intra-BAN communication) during our experiments. These cases represent typical execution of a health telemonitoring application in the MobiHealth system, and they are:

0. WLAN OFF, GPRS OFF
1. WLAN OFF, GPRS ON-ACTIVE
2. WLAN ON-IDLE , GPRS ON-ACTIVE
3. WLAN ON-ACTIVE, GPRS OFF
4. WLAN ON-ACTIVE, GPRS ON-IDLE
5. WLAN OFF, GPRS ON-IDLE
6. WLAN ON-IDLE, GPRS OFF
7. WLAN ON-IDLE, GPRS ON-IDLE

Note: Theoretically, it is also possible to have the WLAN in ON-ACTIVE and GPRS in ON-ACTIVE state; however, because this case is not implemented yet in the MobiHealth system (would require substantial application changes) we have not included it in our study.

Case 0 represents application ‘base’ energy consumption, i.e. for intra-BAN communication and the MBU processing and local storage of application-data (no extra-BAN communication). Additionally to this case, cases 5-7 represent application ‘base’ energy consumption increased of energy consumption for maintaining one (or both) NI in an ON-IDLE state. These cases (5-7) represent



Case No.	NI's Normalized Average Power <sub>MBU</sub> Values	
	Measurement case (Note: BT ON-ACTIVE for all cases)	Normalized power consumption [1/min]
0	WLAN OFF, GPRS OFF	0.00092
5	WLAN OFF, GPRS ON-IDLE	0.00487
6	WLAN ON-IDLE, GPRS OFF	0.00568
7	WLAN ON-IDLE, GPRS ON-IDLE	0.00963
1a	WLAN OFF, GPRS ON-ACTIVE (1.2-1.5 kbps)	0.00721
1b	WLAN OFF, GPRS ON-ACTIVE (5.2 kbps)	0.00874
1c	WLAN OFF, GPRS ON-ACTIVE (7.7 kbps)	0.00897
3a	WLAN ON-ACTIVE, GPRS OFF (1.2-1.5 kbps)	0.00873
3b	WLAN ON-ACTIVE, GPRS OFF (5.2 kbps)	0.00911
3c	WLAN ON-ACTIVE, GPRS OFF (NetPerf, 3.45 Mbps)	0.00982
4a	WLAN ON-ACTIVE, GPRS ON-IDLE (1.2-1.5 kbps)	0.00960
4b	WLAN ON-ACTIVE, GPRS ON-IDLE (5.2 kbps)	0.00974
4c	WLAN ON-ACTIVE, GPRS ON-IDLE (NetPerf, 3.95 Mbps)	0.00947

As we observe from Tab. 1, WLAN in ON-IDLE state consumes comparably the same energy as in ON-ACTIVE state (cases 4a, 7). This can be explained by the Qtek configuration, in which we did not instruct it to get into WLAN *power-save* mode when being ON-IDLE state. In this case, the WLAN NI continuously receives and processes all the data broadcasted between the Access Point and other WLAN devices.

Moreover, we conclude from the Tab.1, that from the power perspective, it is always better to use the GPRS NI and keep the WLAN OFF. If WLAN NI is used, it is always better to keep GPRS OFF.

## 5.2 Application-Data Delay (AppRTT)

We have executed measurements cases as given in Section 4.2 and observed, as we have previously expected, that AppRTT depends on the NI(s) used and the data volume being sent. Tab. 2 summarizes the results, with emphasis on the AppRTT mean value. Note that these results are reported only for the telemonitoring application execution, i.e., not for the cases when we have used the NetPerf.

TABLE II. NI'S APPRTT VALUES

AppRTT [ms] & case No.	NI's AppRTT Values				
	mean	stdev	min	max	med
1a.	3739	2005	1979	20856	3318

AppRTT [ms] & case No.	NI's AppRTT Values				
	<i>mean</i>	<i>stdev</i>	<i>min</i>	<i>max</i>	<i>med</i>
1b.	5505	2627	2767	20702	4706
1c.	6693	3954	2322	28220	5589
3a.	2753	1769	530	23807	2706
3b.	3513	2863	587	36819	3290
4a.	1806	1082	556	15756	1553
4b.	2211	1084	379	13609	2204

As we observe, from the delay perspective, the best is, whenever possible, to use a WLAN ON-ACTIVE and keep GPRS ON-IDLE (cases 4a, 4b). If WLAN is not available and it is necessary to use GPRS, it is better to use lower data volumes (case 1a), or, if patient is not in an emergency, gather the data for a local storage, and send it at the maximum possible volume later over WLAN (case 4b). An interesting observation is that for the real-time application-data sending, the GPRS has higher delay but slightly lower delay variation (i.e. stdev value) comparing to the WLAN (case 1a of 53% vs. 3a of 64% of a mean value). Moreover, the WLAN has lower delay and delay variation when GPRS being ON-IDLE (case 4a) than when GPRS being OFF (case 3a). That may be related to the internal NI management of the mobile device used (the real reasons are unknown for us, and to the best of our knowledge similar results have not been published so far).

### 5.3 NI activation strategies

In this section, we define the *basic* MBU NI activation strategies as ones, in which sending of patient vital signs data is done through an ON-ACTIVE NI in a real-time, i.e., without application-data buffering. These strategies are  $S_{EM}$ ,  $S_1$  and  $S_2$  defined correspondingly to cases 4a, 3a and 1a and are to be used in emergency, but can also be used in non-emergency. These strategies are ordered by their AppRTT in Tab. 3, with the most delay-efficient strategy  $S_{EM}$  (and hence most recommended in emergency) and the least efficient  $S_2$ . The power consumed by the strategy  $S_{EM}$  is considered as our reference point for comparing the power efficiency of other strategies. The power efficiency of strategy  $S_X$  is then defined by  $(\text{power}_{MBU}(S_{EM}) - \text{power}_{MBU}(S_X)) / \text{power}_{MBU}(S_{EM})$ ; the bigger the resulting value, the more efficient the strategy is. The last row in Tab. 3 indicates if the strategy fulfills the requirement of a user being reachable on his/her mobile device via the WWAN-GPRS network.

TABLE III. PERFORMANCE OF THE BASIC NI ACTIVATION STRATEGIES

Strategy	Performance of the Basic NI Activation Strategies		
	$S_{EM}$ (4a)	$S_1$ (3a)	$S_2$ (1a)
AppRTT [ms]	1806	2753	3739
power efficiency	0	9	25

Strategy	Performance of the Basic NI Activation Strategies		
	$S_{EM} (4a)$	$S_I (3a)$	$S_2 (1a)$
WWAN reachability	yes	no	yes

For cases where the larger AppRTTs are acceptable, i.e. in non-emergency, the MBU may adapt application-data flows by acquiring  $n-1$  ( $n>1$ ) seconds of the patient vital signs data, temporarily storing this data, and sending it in a burst in the  $n^{\text{th}}$  second (together with the  $n^{\text{th}}$  second data sample) to the backend-server via a chosen NI. The entries in Tab. 2 and 3 for cases where data volumes achieve 5.2 kbps (1b, 3b, 4b) and 7.7 kbps (1c) make our basis to consider  $n=4$  (thus achieving 5.2 kbps) and  $n=6$  (thus achieving 7.7 kbps).

Tab. 4 summarizes the comparison results for three distinctive application-data flow adaptation cases extrapolated from measurements cases: 1b, 3b, 4b and 1c. The power efficiency of a strategy is again defined against the  $S_{EM}$ . The following relations hold in the Tab.:

$$\text{AppRTT} = (n-1)*1000 + \text{measured AppRTT [ms]}$$

$$\text{Normalized power} =$$

$$1/n [(n-1) \text{power}_{\text{MBU}}(\text{NI}_1=\text{ON-IDLE}, \text{NI}_2=s)$$

$$+ \text{power}_{\text{MBU}}(\text{NI}_1=\text{ON-ACTIVE}, \text{NI}_2=s)]$$

where  $\text{NI}_1$  represents the NI through which the data is sent, while  $\text{NI}_2$  is being in a state  $s$ .

TABLE IV. PERFORMANCE OF THE BASIC NI ACTIVATION STRATEGIES

Strategy	Performance of the Basic NI Activation Strategies			
	$S_4 (4b, n=4)$	$S_5 (3b, n=4)$	$S_6 (1b, n=4)$	$S_7 (4c, n=6)$
WLAN	alternates: ON-IDLE ↔ ON-ACTIVE	alternates: ON-IDLE ↔ ON-ACTIVE	OFF	OFF
GPRS	ON-IDLE	OFF	alternates: ON-IDLE ↔ ON-ACTIVE	alternates: ON-IDLE ↔ ON-ACTIVE
AppRTT [ms]	3000 + 2211	3000 + 3513	3000 + 5505	5000 + 6693
normalized power	0.00966	0.00654	0.00584	0.00555
power eff.	-0.6	32	39	42
WWAN reachability	yes	no	yes	yes

From the Tab. 4 we conclude that for a patient in non-emergency, strategies  $S_6$  and  $S_7$ , where data is sent in burst through the GPRS NI, are more power efficient than those where data is sent through WLAN NI, however less AppRTT-efficient. The result for strategy  $S_4$  shows that this strategy is a bit less power-efficient comparing to  $S_{EM}$ . This is due to the high power consumption of MBU for WLAN ON-IDLE state (as we explained for Tab. 1).

For the cases with larger bursts (i.e. larger  $n$ ), we use the results for NetPerf measurements to extrapolate the efficiency, as presented in Tab. 5. Hereto, we estimate the maximum:

$$\text{AppRTT} \approx (n-1) + C \text{ [s]},$$

where  $C$  is a constant, with a slight dependency on  $n$ , in the order of a few seconds and approximately represents the time of  $n$  data samples. Similarly, the normalized power is computed as:

$$\begin{aligned} &\text{normalized average power} \approx \\ &1/n [(n-1) \text{power}_{\text{MBU}}(\text{WLAN}=\text{ON-IDLE}, \text{GPRS}=\text{s}) \\ &+ \text{power}_{\text{MBU}}(\text{WLAN}=\text{ON-ACTIVE}, \text{GPRS}=\text{s})] \end{aligned}$$

where  $s$  is a given state of the GPRS NI. For large values of  $n$ , the normalized average power approaches the  $\text{power}_{\text{MBU}}$  for (WLAN=ON-IDLE, GPRS= $s$ ) case.

Strategies  $S_8$  and  $S_9$  as defined in Tab. 5, disclose large difference for the WLAN NI alternating between ON-IDLE and ON-ACTIVE states, and GPRS being in ON-IDLE or OFF states. If  $n$  is large enough, one may switch the WLAN NI between OFF and ON-ACTIVE states<sup>8</sup> resulting in strategies  $S_{10}$  and  $S_{11}$ .

TABLE V. PERFORMANCE OF THE BASIC NI ACTIVATION STRATEGIES

Strategy	Performance of the Basic NI Activation Strategies			
	$S8$ (large $n$ )	$S9$ (large $n$ )	$S10$ (large $n$ )	$S11$ (large $n$ )
WLAN	ON-IDLE↔ ON-ACTIVE	ON-IDLE↔ ON-ACTIVE	OFF↔ ON-ACTIVE	OFF↔ ON-ACTIVE
GPRS	ON-IDLE	OFF	ON-IDLE	OFF
AppRTT [ms]	$\approx n-1 + C$	$\approx n-1 + C$	$\approx n-1 + C$	$\approx n-1 + C$
normalized power	$\approx (n-1)/n$ 0.00963	$\approx (n-1)/n$ 0.00568	$\approx (n-1)/n$ 0.00487	$\approx (n-1)/n$ 0.00092
power efficiency	-0.3	41	49	90
WWAN reachability	yes	no	yes	no

As can be seen from the Tab. 5, strategy  $S_{10}$  is slightly more power efficient than  $S_7$  while it induces very large AppRTT. Only the power efficiency of strategy  $S_{11}$  is significantly higher with respect to that of the strategy  $S_7$ , but the drawback is that the mobile device is not WWAN-reachable. The results of Tab. 5, indicate that adapting patient vital signs data and sending it in large bursts (i.e. with a large  $n$ ) is not power efficient enough to motivate having a very long AppRTT or being WWAN-unreachable.

## 6 Related Work

Related work on NI activation strategies is mainly theoretical, and moreover focuses mainly on applications in which mobile user acts as an occasional data consumer and does not produce data, as in the MobiHealth system. For example, authors of [10-13] consider NI strategies together with methods for local or proxy-based caching data for users of email application and web-services. The work reported in [14] reduced energy consumption by introducing a NI ON-IDLE stand-

<sup>8</sup> These NI state changes impose a fixed power penalty higher than that in case of strategies  $S_8$  and  $S_9$ . This penalty is negligible as  $n$  increases.

by state, at which the mobile device is wakened-up if there is an incoming network event, e.g. a call. Considering the impact of applications on NI power consumption, the authors of [15] studied the WLAN NI energy consumption for different multimedia data streaming applications like Microsoft (Windows media), Real (Real media) and Apple (Quick Time) content. They considered only WLAN NI and downlink data streams. Similarly, but from the NI perspective, authors of [16] measured NI energy consumption of use/and alternating between BT and WLAN NIs for a multimedia content download. Furthermore, there exist general research frameworks, in which NI activation strategy is considered as one of multiple features. For example, the research reported in [17, 18] considered a simultaneous operation of NIs in multi-homed mobile hosts, and introduced a Basic Access Network to carry out signalling for network discovery, NI selection, inter-network handover, location updates, paging, authentication, authorization, and accounting. Authors tackled the NI activation strategy objective only theoretically. Similarly, the theoretical framework proposed in [19] focuses specifically on the WLAN NI activation strategy, based on the WLAN network availability, network state (throughput, delays and reliability), as well as application QoS requirements. Their NI strategy assumes that the UMTS network is always ON and available. However, they do not consider the NI energy consumption in their framework. Authors of [20] aimed to estimate WLAN network availability and conditions without powering a NI up - based only on historical data. They have simulated healthcare application by data for 3 leads ECG; however they neither include BT power consumption for sensor-set nor adapted application-data flow being sent by network (i.e. it was fixed at 5 minutes). And finally, in our previous work [21], we have studied the NI activation strategies based on its relative energy cost. We measured energy costs while sending dummy TCP packets over a given NI. However, the data range send was 25 kbps (GPRS) and 2 Mbps (WLAN), and the mobile devices, as well as measurements conditions were different, which made these results unusable for the MobiHealth case study presented in this paper. We emphasize the contribution of our research as an extensive case study of the existing system for telemonitoring of patient's health conditions, based on which we provide extensive and valuable recommendations for the system users.

## 7 Conclusions and the MobiHealth System Recommendations

Based on our measurements, we derive some conclusions and recommendations for the MobiHealth system and its cardiac telemonitoring application, concerning the most efficient and effective NI activation strategies along the power and the delay QoS requirements. Particularly, we have observed that the GPRS and WLAN NIs have complementary power and delay profiles. For GPRS, there is lower energy cost to maintain connectivity and lower energy to send data, but higher delay. On the other hand, the energy cost of a WLAN data send can be higher, but delay is lower. Minimal power is used in strategies where data is stored and sent later it bursts ( $S_8$ - $S_{11}$ ), resulting in the highest delay (as they include long local storage time). Maximum power is used by  $S_{EM}$  (comparing to the other strategies where data is sent in real-time:  $S_1$  and  $S_2$ ), while the delay is minimal.

In an emergency case, the WLAN ON-ACTIVE and GPRS ON-IDLE NI activation strategy should be used, as it provides the system with the lowest patient vital signs data delay. However, if WLAN is not available, GPRS ON-ACTIVE and WLAN-OFF case should be used.

In non-emergency, when the user needs to be reachable, the data can be sent in burst and power needs to be optimized, we recommend the use of the WLAN ON-ACTIVE and GPRS ON-IDLE strategy. The recommended burst size is the one corresponding to  $n=4$  seconds of patient vital signs data. However, if WLAN is not available, GPRS should be used with WLAN OFF with a recommended burst size corresponding to  $n=6$  seconds patient vital signs data.

Another conclusion derived from our studies is that the device used as the MobiHealth's MBU – Qtek 9090 is not necessarily the best choice from the power efficiency perspective for GPRS/WLAN interfaces. As one of the future work areas, we recommend execution of measurements for other devices, and comparison of results between the studies.

Moreover, future work encompasses work on more elaborated NI activation strategies methods, e.g. those including multiple periodic application-data flows with different delay requirements (i.e. different delay defined per application-data flow). Moreover, the NI strategy should include network's monetary cost usage and a network's security level required by the MobiHealth users. Finally, we plan to extend our study of the power- and delay application-data flow adaptation from the user's stationary position to different mobility levels, where data is sent over the different WWAN networks (GPRS, UMTS, or HSPA) as available at a given user's geographical location and time.

## References

- [1] Tachakra, S., X. Wang, et al. Mobile e-Health: the Unwired Evolution of Telemedicine. *Telemedicine J and e-Health*, 2003, 9(3): 247-257.
- [2] van Halteren, A., Bults, R., et al. Mobile Patient Monitoring: The MobiHealth System. *The Journal on Information Technology in Healthcare*, 2004, 2(5): 365-373.
- [3] Dokovsky, N., A. van Halteren, et al. BANip: Enabling Remote Healthcare Monitoring with Body Area Networks. Intl Workshop on Scientific Engineering of Distributed Java Applications (FIJI03), 2003, Luxembourg, Springer Verlag.
- [4] Pawar, P., van Beijnum, B. J., et al. Context-Aware Middleware Support for the Nomadic Mobile Services on Multi-homed Handheld Mobile Devices. *IEEE Symp. on Comp. & Comm.*, Portugal, IEEE, 2007
- [5] Wac, K., Bults, R., et al. Mobile Health Care over 3G Networks: The MobiHealth Pilot System and Service. *Global Mobile Congress*, Shanghai, China, 2004.
- [6] Broens, T., Huis in't Veld, R., et al. Determinants for successful telemedicine implementations: a literature study. *Journal for Telemedicine and Telecare*, 2007, 13(6): 303-309.
- [7] Bernaschi, M., Cacace, F., and Iannello, G. Vertical Handoff Performance in Heterogeneous Networks. Intl Conf. on Parallel Processing Workshops (ICPPW04), 2004, Montreal, Canada.
- [8] Twente Medical Systems Intl., [www.tmsi.com](http://www.tmsi.com), retrieved on 09/12/2007.
- [9] Netperf homepage: [www.netperf.org](http://www.netperf.org), retrieved on 25/11/2007.

- [10] Flinn, J. and Satyanarayanan, M. Energy-aware adaptation for mobile applications. *ACM Symp. on Operating Systems Principles*, USA. ACM, New York, NY, 48-63., 1999.
- [11] Armstrong, T., Trescases, O., Amza, C., and de Lara, E. Efficient and transparent dynamic content updates for mobile clients. *MobiSys'06*, Sweden. ACM, NY, US, 56-68, 2006.
- [12] Lufei, H. and Shi, W. e-QoS: energy-aware QoS for application sessions across multiple protocol domains in mobile computing. *QShine'06*, Canada. v.191. ACM, New York, NY, 2006.
- [13] Anand, M., Nightingale, E. B., and Flinn, J. Self-tuning wireless network power management. *Wirel. Netw.* 2005, 11(4), 451-469.
- [14] Shih, E., Bahl, P., and Sinclair, M. J. Wake on wireless: an event driven energy saving strategy for battery operated devices. *MobiSys'02*, USA. ACM, New York, NY, 160-171, 2002.
- [15] Chandra. S., Wireless network interface energy consumption. Implications for popular streaming formats, *Multimedia Systems*, Springer-Verlag, 9(2), pp. 185-201, 2003.
- [16] Pering, T., Agarwal, Y., Gupta, R., and Want, R. *CoolSpots*: reducing the power consumption of wireless mobile devices with multiple radio interfaces. *MobiSys'06*, Sweden. ACM, US, 220-232, 2006
- [17] Inoue, M. Mahmud, K., Murakami, H. Hasegawa, M. and Morikawa, M. Novel Out-of-Band Signaling for Seamless Interworking Between Heterogeneous Networks, *IEEE Wireless Comm.* 2004
- [18] Wu, G., Mizuno, M. and Havinga, P. MIRAI Architecture for Heterogeneous Network, *IEEE Comm. Magazine*, Feb 2002.
- [19] Song, Q. and Jamalipour. A. Network Selection in an Integrated Wireless LAN and UMTS Environment Using Mathematical Modeling and Computing Techniques. *IEEE Wireless Comm.*, 12(3), 2005, 42-48.
- [20] Rahmati, A. and Zhong, L. Context-for-wireless: context-sensitive energy-efficient wireless data transfer. *MobiSys'07*, Puerto Rico. ACM, New York, NY, 165-178, 2007
- [21] Bargh, M., A. Peddemors. Towards an Energy-Aware Network Activation Strategy for Multi-Homed Mobile Devices. *Intl Conf. on Pervasive Systems Computing*, USA, 2006